#### **1st Symposium on Theranostics** Cracow, 9-11 October 2021

# Metabolic and Positronium Imaging sensitivity of the Total Body J-PET tomographs

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On behalf of the J-PET Collaboration

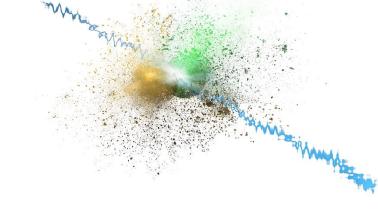




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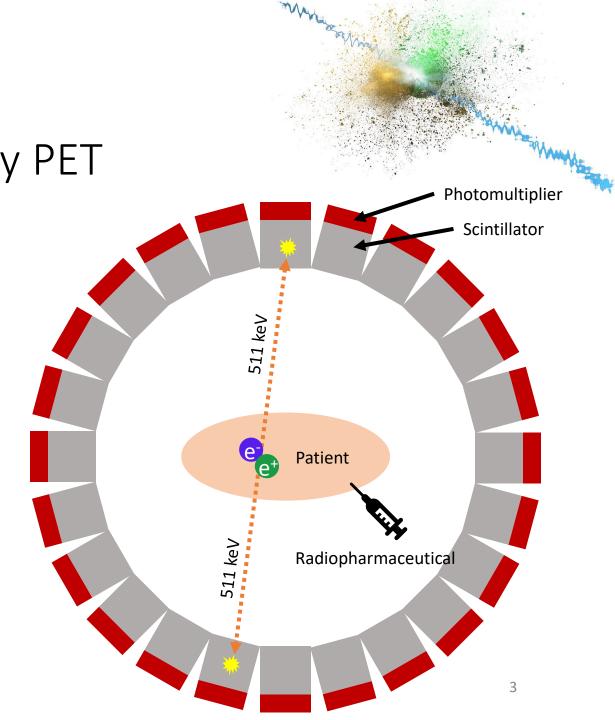
# Outline

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#### Introduction Positron Emission Tomography PET

- One of the most technologically advanced diagnostic methods
- Allows for non-invasive study of physiology, metabolism, and molecular pathways in the human body
- The principle of operation is based on the detection of pairs of gamma quanta



### Introduction Metabolic and Positronium Imaging

Metabolic Imaging

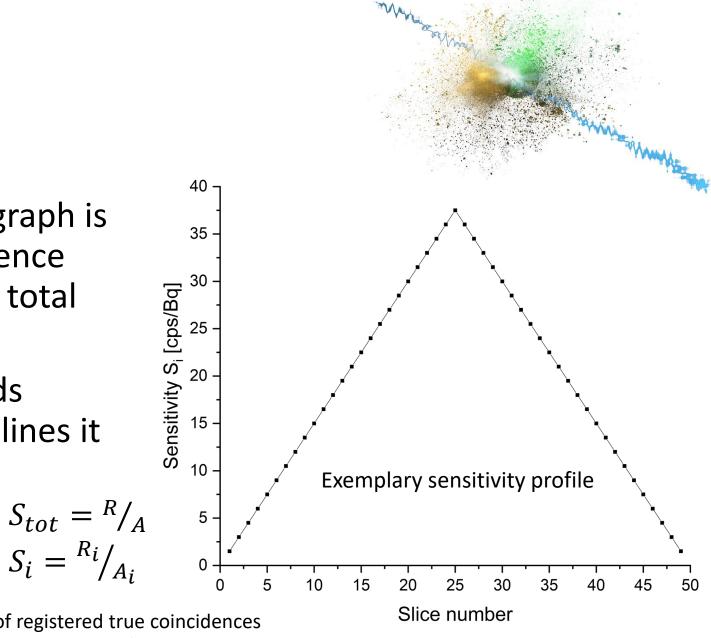
- Standard imaging in PET systems
- Based on the back-to-back annihilation photons
- Enables diagnosis of the uptake of radiopharmaceuticals in cells (SUV)

**Positronium Imaging** 

- Complementary to Metabolic
- Based on the back-to-back annihilation photons and deexcitation gamma
- Ortho-Positronium mean lifetime instead of SUV parameter
- Enables imaging of the inner structure of tissues
- Additional diagnostic indicator

#### Introduction Sensitivity

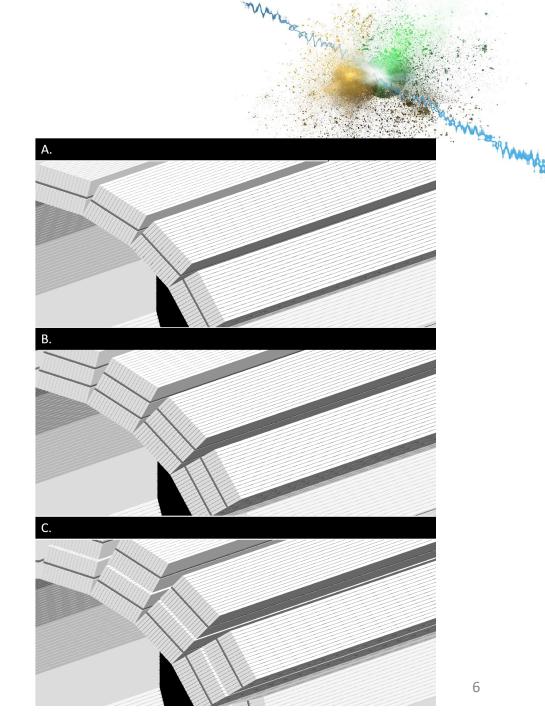
- The sensitivity of a PET tomograph is expressed as the true coincidence events rate normalized to the total activity of the source
- According to "NEMA Standards Publication NU 2-2018" guidelines it can be reported as:
  - System (total) sensitivity
  - Sensitivity profile, where



### Methods

Tomographs designed with J-PET technology:

- Scintillator material plastic (EJ230, Eljen Technology)
- Axial arrangement
- Silicon photomultiplier (SiPM) readout at both ends
- Three designs were taken into account:
- A. 2 panels × 16 scintillators
- B. 3 panels × 16 scintillators
- C. 4 panels × 16 scintillators



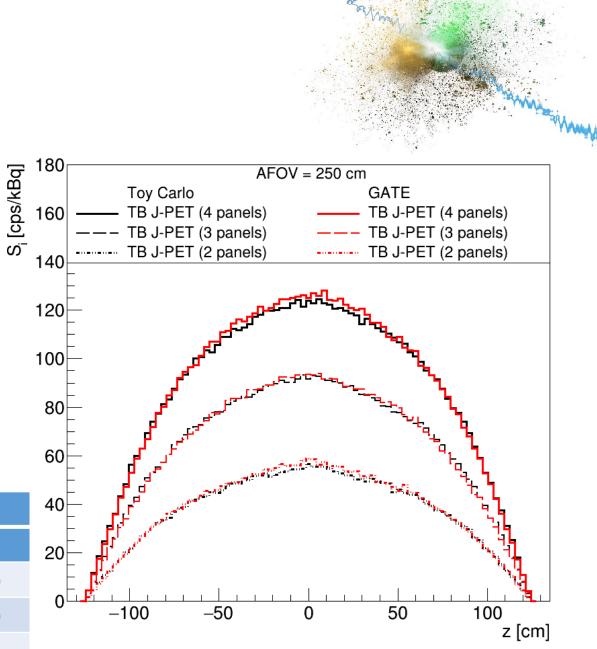
### Methods

Presented study was conducted with a use of a dedicated Toy Monte-Carlo model:

- event-by-event basis
- true coincidence registration
- Metabolic and Positronium Imaging

Validation was performed as a comparison with the standard GATE software

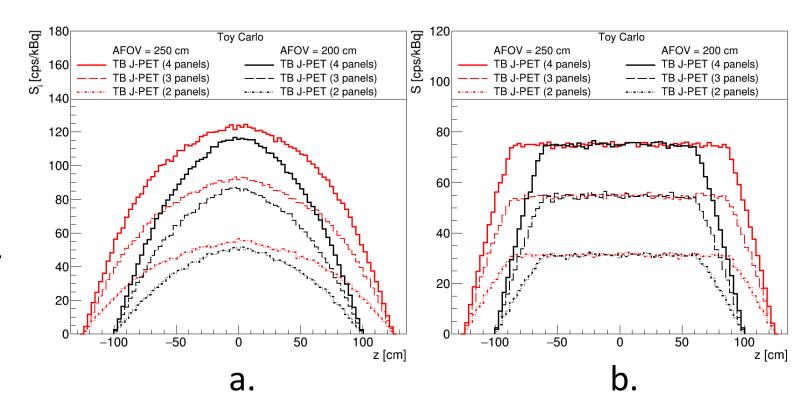
Design	S <sub>tot</sub> [cps/kBq]	
	Toy Carlo	GATE
Α.	37.14(06)	36.46(06±07)
В.	62.12(08)	62.21(08±08)
C.	85.47(09)	84.7(0.9±1.1)



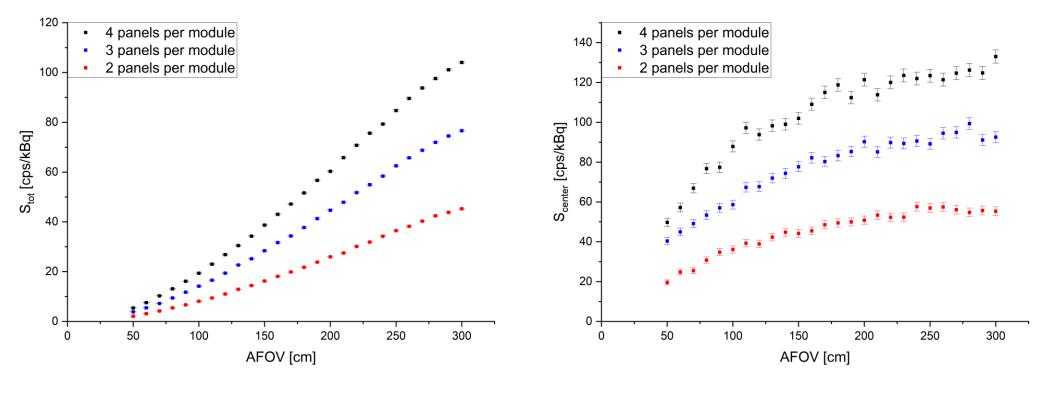


Sensitivity profiles of the 200 cm and 250 cm long (AFOV) Total Body J-PET tomographs:

- a. without any conditions
- b. with imposed angular acceptance criterion on 45° angle

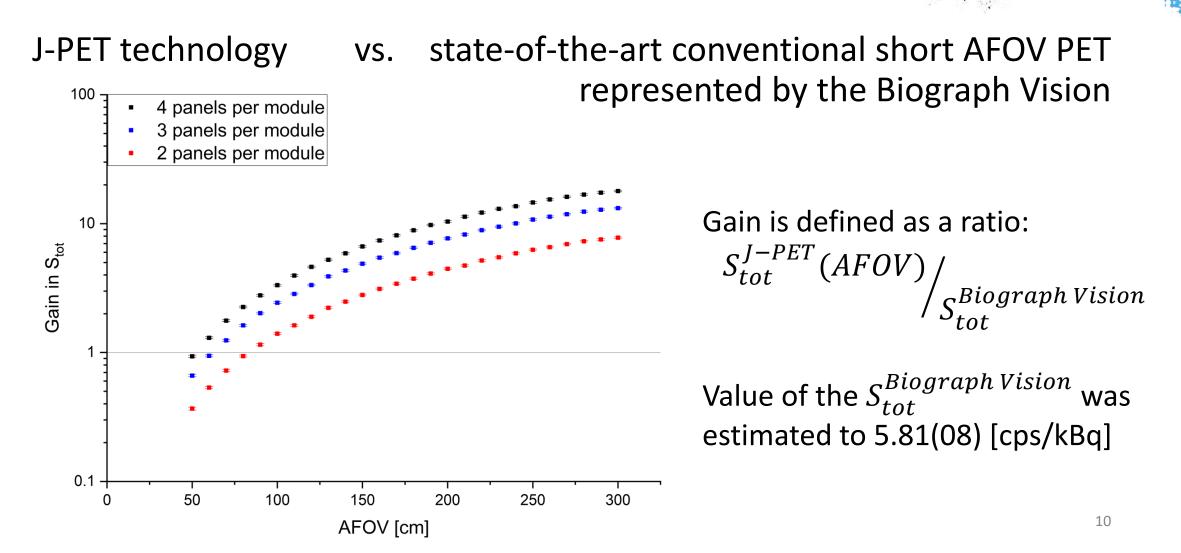


Dependence of the sensitivity on the PET scanner's length



System (total) sensitivity

Sensitivity in the center of PET scanner

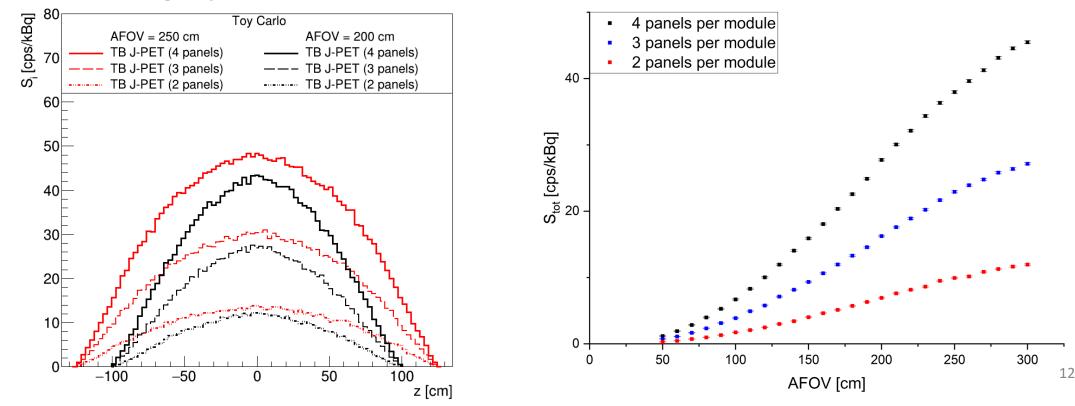




For the study of Positronium Imaging a <sup>44</sup>Sc isotope was chosen as a radioisotope. A corresponding reaction chain of  $\beta^+$  decay:  ${}^{44}Sc \rightarrow {}^{44}Ca^* + e^+ + \nu \rightarrow {}^{44}Ca + \gamma + e^+ + \nu$ 

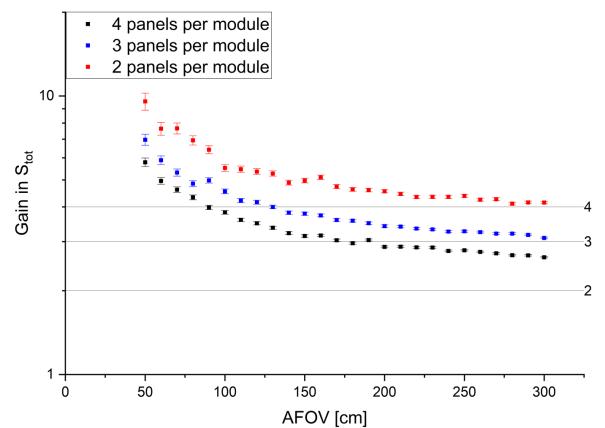
creates excited <sup>44</sup>Ca\* nucleus, which during the deexcitation process emits prompt photon of 1160 keV energy

Sensitivity profiles of the 200 cm Dependence of the sensitivity on and 250 cm long (AFOV) Total Body the PET scanner's length J-PET tomographs



VS.

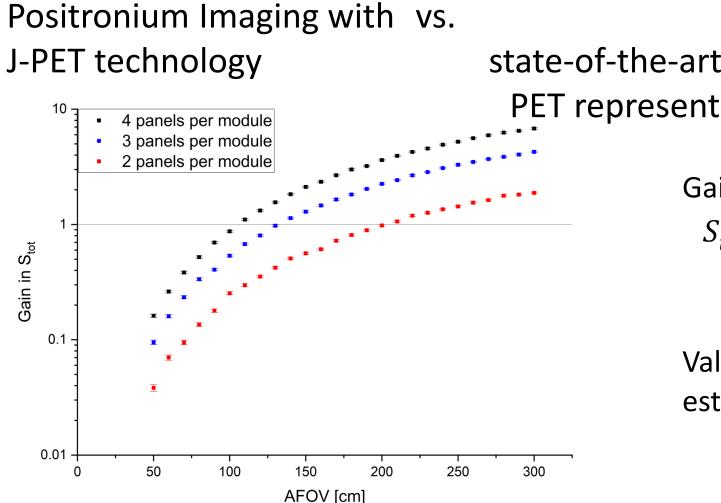
Metabolic Imaging with J-PET technology



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Positronium Imaging with J-PET technology

Gain is defined as a ratio:  $S_{tot}^{Metabolic}(AFOV) / S_{tot}^{Positronium}(AFOV)$ 



Metabolic Imaging with state-of-the-art conventional short AFOV PET represented by the Biograph Vision

> Gain is defined as a ratio:  $S_{tot}^{J-PET}(AFOV) / S_{tot}^{Biograph \, Vision}$

Value of the  $S_{tot}^{Biograph Vision}$  was estimated to 5.81(08) [cps/kBq]

## Summary

#### **Metabolic Imaging**

- System sensitivity up to 84.7(0.9±1.1) [cps/kBq]
- Sensitivity at scanner's center up to 124.1(1.0±1.1) [cps/kBq]
- Uniform simultaneous sensitivity over the patient's body
- Up to ~15 times improvement with respect to conventional short AFOV tomographs

#### **Positronium Imaging**

- System sensitivity up to 30.63(06±31) [cps/kBq]
- Sensitivity at scanner's center up to 48.37(64±60) [cps/kBq]
- Only ~3 times worse than Metabolic Imaging
- Up to ~5 times improvement with respect to conventional short AFOV tomographs with Metabolic Imaging



#### Acknowledgements

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## References

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# Thank you for your attention

# Dependence of the sensitivity on the PET scanner's length after angular acceptance cut

